

# A Fully Automatic Algorithm for the Analysis of Heart Rate Changes and Cardiac Recovery during Exercise

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## Abstract

*Exercise test is a challenging experimental condition for signal processing tools since stationarity requirement is not fulfilled.*

*The aim of the present study was to develop a new way to look at HR and RR variability in exercise test, focusing both on exercise and the subsequent recovery phase.*

*From RR series, the first derivative of the filtered tachogram and the variance were calculated in windows of predefined length and the three experimental conditions (rest, exercise and recovery) were automatically detected.*

*Results indicate that in healthy subjects variance is larger during recovery than during exercise for a given RR interval, this is not seen in heart failure patients. In healthy subjects tonic and dynamical control of heart rate should be regarded as different autonomic regulations.*

## 1. Introduction

The Post-exercise heart rate (HR) recovery and HR variability are commonly used non-invasive assessment procedures for determination of cardiovascular autonomic function.

A delay in HR recovery has been observed in patients with chronic heart failure

Studies of the electrocardiogram during and after exercise (walking on a treadmill ergometer at standard speed and grade) in normal subjects have been performed for very long time [1, 2].

Several techniques have been used varying from the analysis of heart rate variability [3] prior and after exercise, Poincaré [4] plots to the analysis of heart rate (HR) sudden increase [5, 6] and other HR changes [7] with exercise and HR recovery after exercise [8-10].

Normal subjects as well as several pathologies have been subjected to exercise test

In the field of sport testing, heart rate variability analysis has been used to evaluate modifications of autonomic cardiovascular functions during exercise or

after a training period.

Exercise test is a challenging experimental condition for signal processing since it is a non static process.

In this study we present a new way to look at exercise testing where information on HR recovery and HR variability changes are presented simultaneously.

## 2. Methods

### Study Population

Our study includes 10 heart failure (CHF) patients, five of which were females and 12 healthy controls (C).

All subject attended an initial rest-test that was used for validating the healthy/heart failure condition.

On the day of the recording, subjects were recorded at standing resting position for almost five minutes, then in walking condition for an additional 3 minutes. At this point the exercise submaximal test, following a Bruce protocol, took place. Finally, within 30 s from the end of the exercise phase, subjects were positioned in supine position, to start the recovery phase, which was approximately 5 minutes long.

### Algorithm description

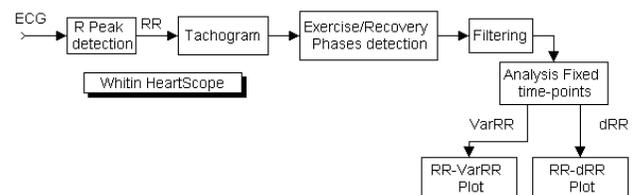


Figure 1. Block diagram of the various signal processing steps undertaken in the study. Detailed description is offered in Methods chapter.

ECGs were recorded during exercise with MP150 data acquisition systems (BIOPAC Systems Inc, Goleta, CA). From the recorded ECGs, RR series were automatically extracted within HeartScope (AMPS Ilc, New York, NY)

[11], software that allows the analysis of cardiovascular signals, from the lead that presented tallest R-waves.

From RR series, the three experimental conditions (rest, exercise and recovery) were automatically detected.

The tachogram was then filtered by a MA filter with a window size of 20 subsequent RRs ( $F_{RR}$ ). Afterwards  $F_{RR}$  was once more filtered with a derivative filter to obtain  $dF_{RR}$ .

The following step was averaging  $dF_{RR}$  series at fixed time points (4s resolution) with a MA filter and the computation of the variance of predefined windows at the same fixed time points of the tachogram to obtain  $Var_{RR}$ .

For comparison purpose, RR and both  $dF_{RR}$  and  $Var_{RR}$  were normalized ( $Var_{RRn}$  and  $dF_{RRn}$ ) using maximum and minimum values.

The final step of the algorithm is the quantification of the area in the phase plane (RR -  $Var_{RR}$ ) and (RR -  $dF_{RR}$ ).

For statistic analysis, nonparametric Kruskal-Wallis test on median was used, p-value<0.05 (\*) was considered significant level, p-value<0.1 (†) was also marked.

### 3. Results

Both exercise and recovery phases present large differences in the two studied populations.

Automatically extracted exercise phases were  $398 \pm 180$  and  $431 \pm 252$  seconds long, while recovery phases were  $193 \pm 78$  and  $160 \pm 61$  seconds long for C and CHF respectively.

As reported in Table 1, time-domain parameter such as maximum HR at exercise peak was significantly higher in healthy individuals, so for  $\Delta RR$  at 80s into recovery phase: HR recovery is almost twofold for healthy, although significance is not reached.

Our new developed parameters on phase-plane analysis present markedly higher values for healthy subjects, precisely  $Var_{RR}$  during the recovery phase (after 40 s from beginning of recovery) was almost two fold in C than CHF.

The observation of Fig 2 and 3 gives an overview of the analysis on phase-plots. For healthy subjects, the variance in the recovery phase is much higher than the exercise phase or rest state.

The trajectories on the phase-plot in heart failure patients were totally perturbed, the monotonic behavior of the initial phase of the recovery was modified to an oscillating pattern.

Table 1. Several analyzed parameters for the two studied population. Results are given as mean  $\pm$  std. Kruskal-Wallis test: (\*) p-value<0.05, (†) p-value<0.1.

	CHF (n=10)	H (n=12)	p-value
Age	67 $\pm$ 11	39 $\pm$ 12	*
Gender (F)	50%	17%	
HR at peak Exercise (bpm)	118 $\pm$ 16	172 $\pm$ 17	*
$\Delta RR$ at 80s in rec. (ms)	110 $\pm$ 57	203 $\pm$ 148	†
$Var_{RR}$ at 80s in rec. ( $ms^2$ )	1507 $\pm$ 4203	3106 $\pm$ 5813	
$dF_{RR}$ at 80s in rec.	446 $\pm$ 448	1226 $\pm$ 1751	†
$Var_{RR}$ area	67 $\pm$ 148	110 $\pm$ 218	†
$dF_{RR}$ area	7.1 $\pm$ 3.2	33.2 $\pm$ 36.7	*

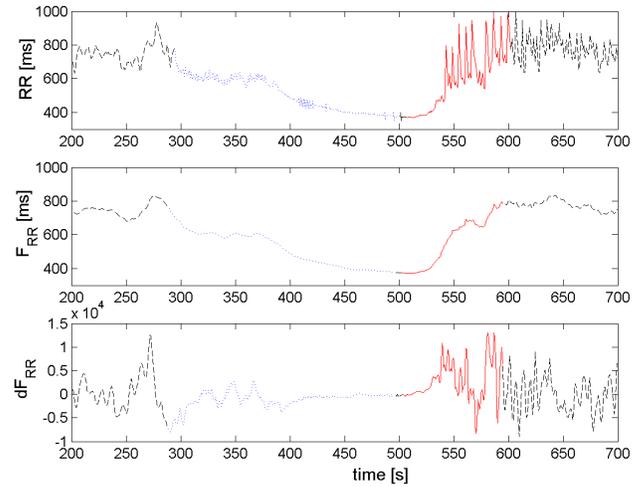


Figure 2. The tachogram, the filtered tachogram and  $dF_{RR}$ -RR for an healthy individual are here shown. The two exercise phases are also visualized differently, dotted line for exercise and solid line for recovery phase. A clear reactivation is visible a minute into recovery phase (sudden RR interval increase and appearance of marked  $dF_{RR}$  oscillations).

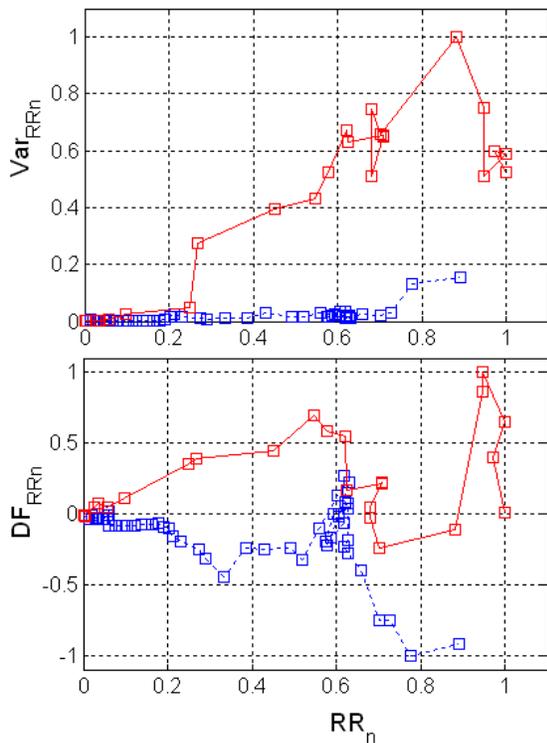


Figure 3. Example of normalized  $\text{Var}_{\text{RR-RR}}$  (upper) and  $d_{\text{RR-RR}}$  (lower) plots for an healthy individual. Time points are 4s apart. It is clear that during the exercise (dotted line) phase  $\text{Var}_{\text{RR}}$  is seriously reduced, while it quickly increases after 20s from the beginning of the recovery (solid line) phase.  $d_{\text{RR}}$  indicates a clear RR decrease during late exercise phase and a monotonic RR increase starting with the beginning of recovery.

#### 4. Discussion and conclusions

The plots clearly indicate that in healthy subjects at a given RR interval the variance is larger during recovery than during exercise and even during rest, thus producing a sort of loop covered clockwise in the phase plane (RR -  $\text{Var}_{\text{RR}}$ ) and (RR -  $d_{\text{RR}}$ ). In healthy subjects the trajectory is not completely closed since the final mean RR interval is significantly larger than that during resting condition. This trajectory collapses onto itself in heart failure patients. These results support the conclusions that:

- i) in healthy subjects tonic control of heart rate, setting the mean value of RR interval, and dynamical control, setting the level of heart rate variability, should be regarded as different autonomic regulations;
- ii) a deeper analysis of the form of the trajectory in the phase plane (RR -  $\text{Var}_{\text{RR}}$ ) and (RR -  $d_{\text{RR}}$ ) during exercise test may unveil important details of the dynamics of cardiac autonomic nervous system

regulation.

Our results should be regarded as preliminary, since age and fitness levels of the examined populations were not matched.

Accordingly, it will be fundamental to validate our findings on a larger and more homogeneous cohort.

This technique might also be useful for quantifying fitness level, analysing groups of healthy subjects before and after physical training.

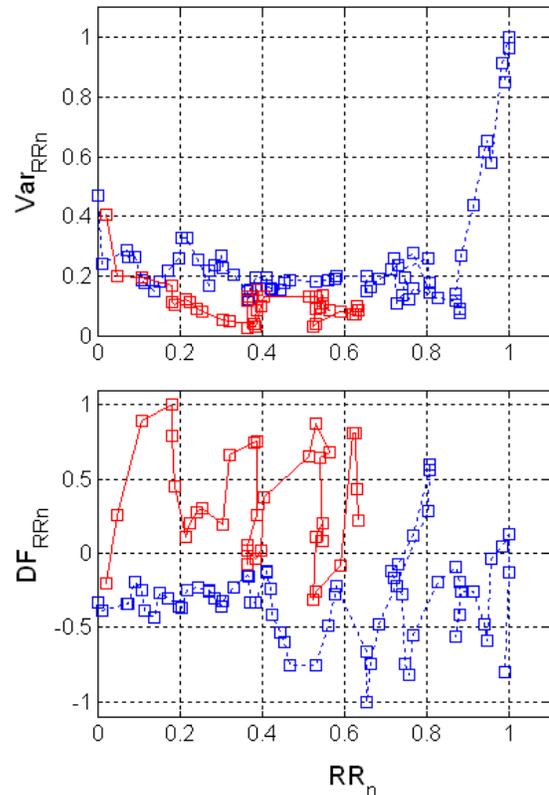


Figure 4. Example of normalized  $\text{Var}_{\text{RR-RR}}$  and  $d_{\text{RR-RR}}$  plots for a CHF subject. Time points are 4s apart. During exercise (dotted line) phase  $\text{Var}_{\text{RR}}$  is reduced, but during recovery (solid line) phase it remains seriously reduced. The process of autonomic recovery is seriously perturbed.  $d_{\text{RR}}$  shows an oscillatory behavior.

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